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The sensor is first flushed with 10 mM HEPES-buffer (pH 7.5) in order to assume the basis line. The one-step activation occurs with a freshly prepared mixture of 100 mM NHS and 400 mM EDC. This solution has a conductivity of 14.4 mS/cm, which is substantially higher than the conductivity of 550 µS/cm of the HEPES buffer. The sensor reacts with a frequency increase of about 100 kHz. Subsequently, the sensor is again flushed with HEPES buffer and then a solution of the biomolecule to be immobilized is applied. The biomolecule - in the present case monoclonal antibodies against urease - is present in a 10 mM acetate buffer at a pH = 5.0. Fig. 2 shows a frequency reduction, which is caused by the mass increase on the sensor surface. From the sensor behavior, the slow adjustment of the equilibrium is apparent which is reached after about 45 to 50 minutes. Then flushing with HEPES buffer takes place again. Subsequently, the excess NHS ester groups are de-activated by ethanolamine. In the last step for the preparation of the biosensor samples 4 mg/ml BSA are applied in order to block the non-specific binding sites.

Amend the claims as follows:

Sub B1
 1. A dextran-coated surface on a carrier having a carrier surface with a connection between dextran disposed as coating on the carrier surface formed by a T-BSA photolinker, said dextran-coating being attached to said carrier surface by co-immobilization of a mixture of the dextran and the T-BSA photolinker.

Sub B2
 3. A dextran-coated surface according to claim 1, wherein said photolinker is a 3-trifluoromethyl-3-(*m*-isocyanophenyl)-diazirine (TRIMID)-modified polysaccharide. ??

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Support?

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